

“ENGINEERING” MECHANICS OF ADHESION OF BIO-CAPSULE AND BIO-MEMBRANE TO A PLANAR SUBSTRATE

Kai-tak Wan (a) and Kuo-Kang Liu (b)

(a) Mechanical & Aerospace Engineering &
Engineering Mechanics, University of Missouri-
Rolla, MO 65409

(b) Tissue Engineering Laboratory, Nanyang
Technological University, Singapore 639798

Abstract

A new theoretical model is presented for the adhesion of a thin-wall capsule onto a planar substrate based on linear elasticity and a simple energy balance. Adhesion of a bio-membrane clamped at the perimeter onto a substrate is also formulated as “punch test”. The new method can be used to investigate thin film adhesion in the presence of specific / non-specific surface forces and chemical environment.

Introduction

Bio-adhesion is an important in many aspects such as metastasis, tissue assembly and drug delivery capsules. In the presence of attractive surface forces, bio-capsule (e.g. liposome) or bio-membrane is drawn to a substrate, deforms elastically until equilibrium is reached. In this paper, we show how “engineering mechanics” is applied to model the adhesion and delamination processes of (i) spherical micro-capsule adhered onto a planar substrate in the presence of osmosis [1], and (ii) a new axisymmetric “punch test” for in-situ adhesion measurement for ultra-thin bio-membrane [2-3].

Mechanics of capsule adhesion

A few assumptions are needed for modeling: (i) capsule wall allows only film stretching; (ii) enclosing liquid is *incompressible*; (iii) adhesion forces are effective only upon direct contact; (iv) visco-elasticity, thermal undulations and the surface charge upregulation are ignored. All lengths hereafter are measured in units of original radius, R_0 . The constant volume is $V_0 = 4\pi/3$, and initial surface area $A_0 = 4\pi$. Upon contact with a substrate, the capsule deforms to a truncated

sphere with a radius, R , contact radius, a , and $(a/R) = \alpha = \sin\theta$ (Figure 1). Thus, volume becomes

$$V = \frac{2\pi R^3}{3} \left[1 + \left(1 + \frac{\alpha^2}{2} \right) (1 - \alpha^2)^{1/2} \right] = V_0 \quad (1)$$

and the enlarged surface area (excluding the contact circle),

$$A = 2\pi R^2 [1 + (1 - \alpha^2)^{1/2}] \quad (2)$$

The uniform biaxial membrane strain is roughly

$$\varepsilon = (1/2) [A/(A_0 - \pi a^2) - 1] \quad (3)$$

corresponding to a membrane stress of $\sigma = C \varepsilon$, with C the extensional rigidity (i.e. $Eh/(1-\nu)$ in a linear membrane), h the film thickness, E and ν the elastic modulus and Poisson’s ratio respectively. A capsule initially adhered onto a substrate is now exposed to a dilute solution, giving rise to an internal osmotic pressure and a liquid influx of volume, V_{in} . The resulting volume becomes $V = (1 + \nu)$ and radius $R = (1 + \nu)^{1/3}$ with $\nu = V_{in}/V_0$. A strain energy release rate, G , defined to be

$$G = (1 - \cos\theta) C\varepsilon + C\varepsilon^2 \quad (4)$$

such that equilibrium is reached when $G = W$, the interfacial adhesion energy. Figure 1 shows a/R as a function of ν . In an isotonic solution, the capsule experiences zero osmotic pressure and the contact circle depends only on the adhesion strength. Osmosis leads to a trajectory **ABCD** for $w = (W/C) = 10^{-3}$. At point **A**, the capsule achieves a maximum contact radius at specific adhesion strength. At point **D**, the capsule pinches off the substrate with zero contact. Our new theory agrees favorably with experimental measurement for a variety of liposomes.

Adhesion measurement using a “punch test”

To facilitate holding a thin fragile bio-membrane in place, it is clamped by two rings with radius of central opening, a . A cylindrical punch of radius, a , is adhered to the film via the opening before an external force, F , is exerted to drive a delamination through the adhered interface (Figure 2). Deformation of the film is governed by

$$\kappa \Delta^2 w - \sigma h \Delta w = F \delta(r) \quad (5)$$

with $\kappa = Eh^3 / 12(1-\nu^2)$ the flexural rigidity, and $\delta(r)$ the delta function. Assuming an average uniform membrane stress on the diaphragm and satisfying the boundary conditions ($w(r=c) = w_0$, $w(r=0) = 0$, $w'(r=c) = 0$, and $w'(r=a) = 0$, where c the radius of contact circle), the differential equation was solved analytically yielding the film profile $w(r)$ and mechanical response without delamination $F(w_0)$. For delamination to occur along the film-punch interface, the strain energy release rate, G , is derived from a simple energy balance and the corresponding mechanical response with delamination, $F(w_0)$. The stability of the mechanical system is considered, and it can be shown easily that when $(dw_0/dF) = 0$, the delamination will propagate spontaneously until the punch is completely separated from the film, or a “pull-off”. From linear elasticity, it was shown earlier that the when $(c/a) \approx 0.18$, “pull-off” occurs. The corresponding critical force and punch displacement are also obtained. The analysis was lately extended to pre-stressed films. “Pull-off” occurs within the range of $0.18 = (c/a) = 0.37$, depending on the magnitude of intrinsic membrane stress.

The new method allows adhesion measurement of ultra thin film. When ligand-receptor pairs are deposited on the punch and film, specific adhesion forces can also be measured. By varying the punch and hole dimension (a), the density of the molecular pair can also be measured. One advantage of the new geometry is that measurement of either F or w_0 , and c/a at “pull-off” is sufficient to determine the adhesion energy and intrinsic membrane stress.

Conclusion

We have shown how solid mechanics is applied to construct a theoretical mechanical model for the adhesive contact mechanics of a capsule onto a substrate in the presence of osmosis. Rise in osmotic pressure within the capsule leads to shrinkage in contact area and even lift-off from the substrate. The axisymmetric punch test can be used to quantify the adhesion of an ultra-thin bio-membrane by measuring the critical load, punch displacement and contact radius at “pull-off”.

References

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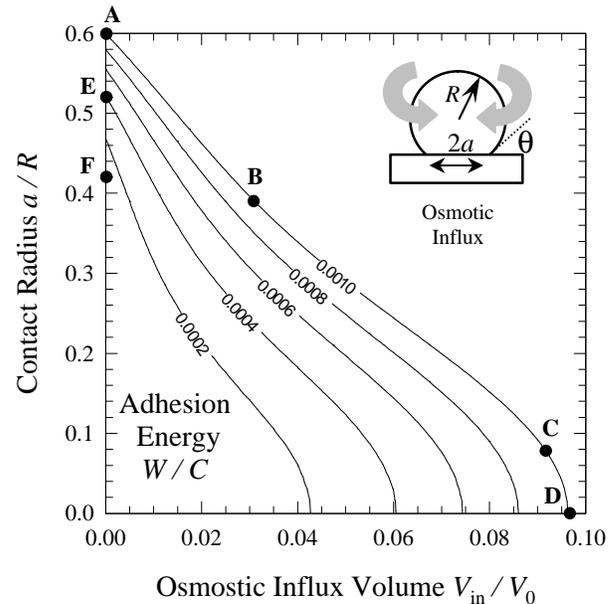


Figure 1. Contact radius as a function of osmotic influx volume. Inset shows the osmotic pressure buildup.

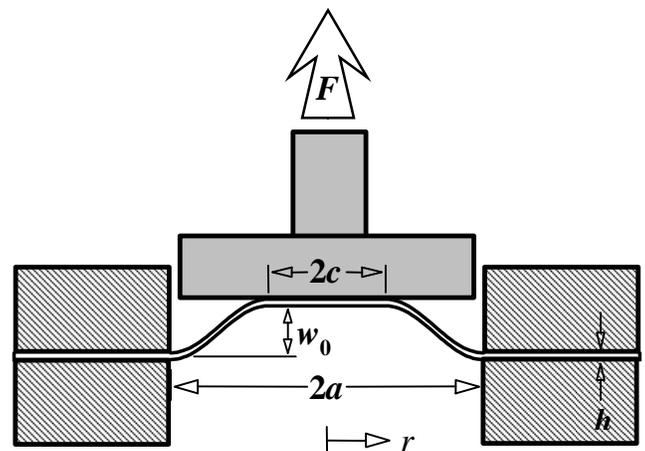


Figure 2. Schematic of axisymmetric punch test. The membrane is clamped by two identical rings with a central opening of radius a .