

# 3-DIMENSIONAL POLYMER-DNA-CALCIUM PHOSPHATE MATRICES FOR NON-VIRAL GENE TRANSFECTION

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## INTRODUCTION

Peptide encapsulated within a biodegradable, polymeric matrix or adsorbed to a polymeric surface has been demonstrated to establish a localized system capable of sustained protein delivery [1,2]; however, polymer processing techniques and *in vivo* implantation have been shown to induce protein unfolding and subsequent inactivity [3]. An alternative strategy to peptide delivery is the delivery of a gene encoding for the factor. Calcium phosphate (Ca-P) mediated gene transfer is an efficient non-viral gene delivery strategy [4]. In this study, we hypothesized DNA/Ca-P co-precipitates could be combined with a 3-dimensional (3D) biodegradable polymeric matrix of poly(lactide-co-glycolide) (PLAGA) to serve as an efficient non-viral gene delivery system. Lambda DNA, which serves as a model DNA, was incorporated into a Ca-P co-precipitate and adsorbed to the surface of a 3D-[50:50] PLAGA (Mw = 63k) scaffold. The release profile demonstrated an initial burst release over the first 48 hours. Cellular transfection by the gene delivery matrix was completed using the osteoblast-like human osteosarcoma cell line, SaOS-2. Cells seeded on the 3D-PLAGA matrix with adsorbed DNA/Ca-P incorporated via endocytosis the DNA within 48 hours as determined by polymerase chain reaction (PCR) analysis. To develop a PLAGA/DNA/Ca-P gene delivery system with a sustained release profile, DNA/Ca-P co-precipitates were incorporated in PLAGA microspheres of [50:50], [75:25] (Mw = 41k), and [80:22] (Mw = 350k) and sintered to form a 3D structure. The release kinetic profile demonstrated these matrices have a significantly reduced initial burst release as compared to the scaffold with adsorbed DNA/Ca-P.

## MATERIALS AND METHODS

**SCAFFOLD FABRICATION** - A modification of the calcium phosphate coprecipitation technique described by Schenborn, et al. [4] was used to fabricate matrices capable of gene delivery. Polymeric matrices with DNA/Ca-P adsorbed to the surface were formed by fabricating microspheres using a solvent evaporation technique and 1% poly(vinyl alcohol) as the emulsifying solution [5]. Microspheres, 425-600  $\mu\text{m}$  in diameter, were placed into a mold and sintered to form

a porous, 3D, matrix. [50:50] PLAGA scaffolds with adsorbed DNA were formed by pipetting the DNA (10 $\mu\text{g}$ )/Ca-P co-precipitates onto the matrices, placing the matrices at -20°C for 24 hours, and vacuum drying for 24 hours. Matrices with DNA (10 $\mu\text{g}$ )/Ca-P incorporated into the microspheres were fabricated by pipetting the co-precipitates into the dissolved polymer and vortexing the mixture for 15 min before pouring into the emulsifying solution.

**RELEASE STUDIES** - Matrices were individually placed in vials containing PBS + 1% antibiotics (pH = 7.4) and incubated in a shaker bath at 37°C. At the appropriate time point, the PBS solution was collected for pH measurement and a colorimetric assay for calcium (Sigma, Kit #578M) was used to quantify precipitate release from the matrices.

**CELLULAR TRANSFECTION** - 3D-PLAGA/Ca-P matrices containing 10 $\mu\text{g}$  of lambda DNA were plated with SaOS-2 cells at a seeding density of 200,000 cells/scaffold. Cells were cultured on the matrices in M-199 supplemented with 10% FBS and 1% P/S for 48 hours and cell lysates collected. Cellular uptake of lambda DNA was confirmed using PCR (Gibco Life Technologies, Kit #11904-018). The sense and antisense primers for lambda amplification are 5'GATGAGTTCGTGTCCGTACACTGG3' and 5'GGTTATCGAAA TCAGCCACAGCG CC3', respectively.

**STATISTICAL ANALYSIS** - A power analysis assuming a 2% standard deviation,  $\alpha=0.05$ , 2 sides, and a power of 0.90 indicated an effect size of 6 matrices per group for the release study. Data is presented as mean  $\pm$  standard deviation.

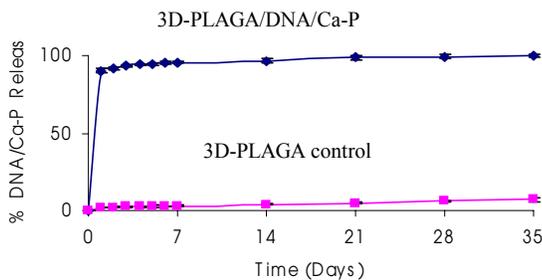
## RESULTS AND DISCUSSION

In these studies, DNA was encapsulated in the Ca-P co-precipitates for adsorption to the polymeric scaffolds or incorporation into the polymeric microspheres. Release studies performed using DNA/Ca-P co-precipitates adsorbed to 3D-PLAGA [50:50] matrices

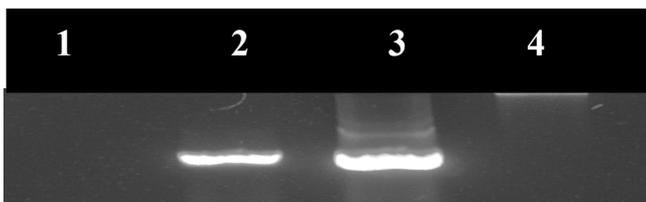
demonstrated an initial burst release, over the first 48 hours (93% release), followed by a slower release over 35 days (Graph A).

To determine the ability of the released DNA/Ca-P co-precipitates to transfect cells cultured on the gene containing matrices, SaOS-2 cells were plated on 3D-PLAGA matrices with adsorbed DNA/Ca-P, cultured for 48 hours, collected, and examined for lambda DNA uptake. PCR analysis verified cellular transfection and the presence of a single band confirmed maintenance of DNA structural integrity (Figure 1).

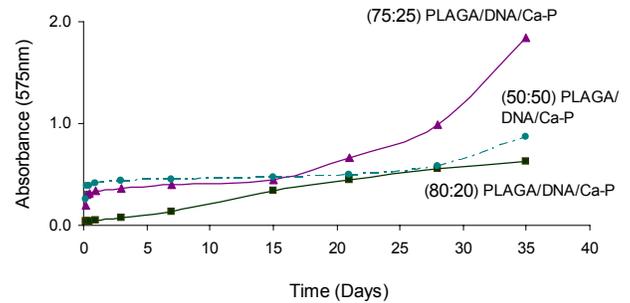
To overcome the rapid initial burst release observed by DNA/Ca-P co-precipitates adsorbed to the 3D-PLAGA matrix surface, an alternative method, which incorporated the DNA/Ca-P co-precipitates into the polymeric microspheres, was developed using PLAGA microspheres of various co-polymer ratios. The release kinetics of these matrices demonstrated a sustained release over 35 days (Graph B). The [50:50] and [75:25] PLAGA/DNA/Ca-P scaffolds demonstrated a reduced initial burst release, as compared to scaffolds with adsorbed DNA/Ca-P, while the [80:20] PLAGA/DNA/Ca-P scaffold had a minimized initial release. The [50:50] and [75:25] PLAGA/DNA/Ca-P matrices demonstrated a steady release until the onset of rapid polymer degradation, indicated by the rapid drop in pH at day 21 (Graph C and D), which subsequently accelerated DNA/Ca-P release. A drop in pH accompanied by an accelerated DNA/Ca-P release was not observed by the matrices fabricated with the higher molecular weight polymer, [80:20] PLAGA (not shown).



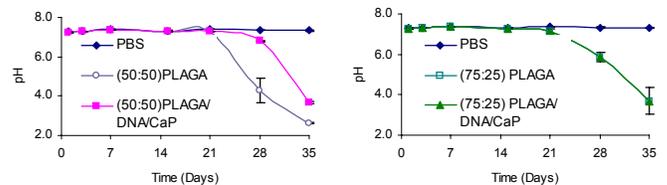
**Graph A: The release profile of DNA/Ca-P co-precipitates adsorbed to 3D-PLAGA scaffolds in PBS, at 37°C. Note the initial burst release over the first 48 hrs. Scaffolds with no DNA/Ca-P served as controls (n=6).**



**Figure 1: PCR analysis for cellular transfection following lambda DNA release from a DNA/Ca-P precipitates adsorbed to the 3D-PLAGA matrix. Lane 1: Negative control for PCR, Lane 2: SaOS-2 cells transfected with lambda DNA released from a 3D-PLAGA/DNA/Ca-P matrix, Lane 3: Lambda DNA (positive control) Lane 4: Non-transfected SaOS-2 cells (negative control)**



**Graph B: Release profile of DNA/Ca-P co-precipitates incorporated in 3D-PLAGA scaffolds of various co-polymer ratios and molecular weights (n=6). Note the rapid initial burst release by DNA/Ca-P co-precipitates adsorbed to the polymer surface (Graph A) is absent.**



**Graph C and D: pH of the PBS degradation solution following incubation with 3D- [50:50] and [75:25] PLAGA/DNA/Ca-P scaffolds. Note the rapid drop in pH of the matrices at day 21 corresponds to the rapid release of DNA/Ca-P observed in the release profile (Graph B).**

## CONCLUSIONS

As the use of naked plasmid DNA delivery is impaired by its low cellular transfection efficiency and susceptibility to nuclease degradation, we present here the first studies to develop a novel, non-viral gene delivery system by combining DNA containing calcium phosphate co-precipitates with a biodegradable, polymeric matrix. Release studies of the adsorbed DNA/Ca-P co-precipitates demonstrate a rapid initial burst release, while DNA/Ca-P co-precipitates incorporated within polymeric microsphere matrices demonstrate a controlled, sustained release. PCR analysis verified the ability of the released DNA containing co-precipitates to transfect SaOS-2 cells cultured on the scaffold. Under controlled conditions, we have found these matrices suitable for non-viral gene therapy strategies. Future studies will examine the transfection efficiency of the DNA/Ca-P co-precipitates incorporated within the 3D-PLAGA microsphere matrix.

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